

A Constructive Evaluation of Medical Image Processing

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Abstract: *A interdisciplinary study field that draws talents from applied mathematics, computer sciences, engineering, statistics, physics, biology, and medicine, biomedical image processing has witnessed enormous development. The use of computer-aided diagnostic processing is already extensively employed in clinical practice. More issues develop as a consequence of the fast growth of high technology and the usage of multiple imaging modalities. One such problem is processing and analyzing a substantial volume of photos in order to give high-quality data for the diagnosis and treatment of illnesses. This course aims to introduce students to the fundamental ideas and methods of medical image processing while igniting their interest in the field's future study and investigation. Both mankind and the entire civilization have gained from the speedy growth of medical research and the production of various pharmaceuticals. Additionally, improvements in contemporary science have been achieved in the surgical profession. However, the most critical prerequisite prior to treatment is a clear and correct diagnosis of the ailment. More sophisticated bioinstruments will enable more accurate diagnosis. The medical picture is crucial to clinical diagnosis, doctor treatment, education, research, and other endeavors. A common misconception about medical imaging is that it uses magnetic resonance imaging and X-ray computed tomography to depict the body's anatomical features. However, it is often more helpful for physiologic function than anatomy. Medical imaging has had a significant impact on the medical industry with the advancement of computer and image technologies. Medical image processing has gained popularity since the quality of medical imaging influences diagnosis. Clinical applications that want to save and retrieve pictures for later use need a practical method to store such images in detail.*

Keywords: Medical Image Processing, Image Segmentation, Feature Extraction.

I. INTRODUCTION

An interdisciplinary field of study known as biomedical image processing brings together specialists in applied mathematics, computer sciences, engineering, statistics, physics, biology, and medicine. Computer-aided diagnostic processing is already extensively employed in clinical practice. The usage of several imaging modalities and the quick development of high technology cause a rise in issues. One such problem is the processing and analysis of a huge number of images to provide high-quality information for the diagnosis and treatment of diseases. While exposing them to the fundamental ideas and methods of medical image processing, this course aims to pique students' interest in the field's ongoing investigation and study. There are often reviews of new advances in biological signal processing and image processing [21, 35, 36]. These review articles often provide methods for working with pixel and voxel data, including image segmentation, or how to utilize them for diagnosis, treatment planning, and follow-up studies. Contrarily, the emphasis of this study is on the challenges associated with processing substantial volumes of medical imaging data. Medical image data ranging from Kilobytes to Terabytes has been produced during the last several years. This is mostly due to improvements in medical image capturing technology, which have led to greater pixel resolution and speedier reconstruction processing. For instance, the most recent Sky Scan 2011 x-ray nano-tomograph has a resolution of 200 nm per pixel whereas the high resolution micro computed tomography (CT) reconstructs images with 8000 8000 pixels per slice and 0.7 m isotropic detail detectability. Each slice results in the production of 64 Megabytes (MB). In modern CT and MRI systems, it is possible to scale both the image resolution and reconstruction time. Full-

body scans of a person at this resolution might provide many Gigabytes (GB) of data. A large amount of image data from a single data set, such in picture archiving and communication systems (PACS), or a considerable amount of image data from hundreds of photographs are the two primary categories of significant medical image data.

Background

We first define terminology that is used throughout the review, and we describe important issues in the segmentation of medical images.

Definitions

A image is a collection of measurements made in two or three dimensions. These measurements in medical images, which are sometimes referred to as "image intensities," may include the radiofrequency (RF) signal amplitude in MRI, the acoustic pressure in ultra sound, or the radiation absorption in X-ray imaging. If just one measurement is made at each location in the image, the image is said to be a scalar image. Medical imaging has undergone a revolution in the past 10 years thanks to the development of technology that is faster, more accurate, and less invasive. Due to this, software development in this area has become necessary, which has substantially expedited the creation of new techniques for signal and image processing. The majority of this overview study will focus on partial differential equations and curvature-driven flows, which are the foundations of many of these techniques. Mathematical modeling is the cornerstone of biomedical computers. Such models must be based on data extracted from images in order to further experimental, clinical, biological, and behavioral research. Modern medical imaging techniques go well beyond the visible light photographs and microscope images of the early 20th century, including all biological scales. Modern medical images may be seen as geometrically arranged collections of data samples that track a number of physical processes, including the diffusion of water molecules through and within tissue and the temporal fluctuation of hemoglobin deoxygenation during brain metabolism. Because of the expanding range of imaging as a tool for organizing our observations of the biophysical world, our capacity to use new processing techniques and combine data from various channels into sophisticated and complex mathematical models of physiological function and dysfunction has significantly increased. The creation of biomedical engineering ideas based on solid mathematical foundations is one key subject of research in order to provide general-purpose software approaches that may be integrated into complete treatment delivery systems. Radiation treatment, minimally invasive surgery, and biopsy are just a few image-guided procedures that may be administered more effectively because to such technology.

Types

The two kinds of image processing methods are analog and digital. Image processing techniques for tangible copies like prints and photographs may be analog or visual. Image analysts employ a number of interpretive pillars while implementing these visual methodologies. The image processing is dependent both on analyst skill and the area that has to be explored. Association is a critical component of image processing that uses visual techniques. Analysts use their own knowledge with additional data to assess photographs.

Digital processing techniques are used to enable computer-based digital image editing. due to errors in the image sensors' raw data from the satellite platform. In order to correct these flaws and achieve uniqueness, information must go through a variety of processing phases. All types of data must go through the three primary stages of pre-processing, augmentation and display, and information extraction when using a digital approach..

Fundamental steps in image processing:

1. Image acquisition: to acquire a digital image
2. Image preprocessing: to improve the image in ways that increases the chances for success of the other processes.
3. Image segmentation: to partitions an input image into its constituent parts or objects.
4. Image representation: to convert the input data to a form suitable for computer processing.
5. Image description: to extract features that result in some quantitative information of interest or features that are basic for differentiating one class of objects from another.
6. Image recognition: to assign a label to an object based on the information provided by its descriptors.

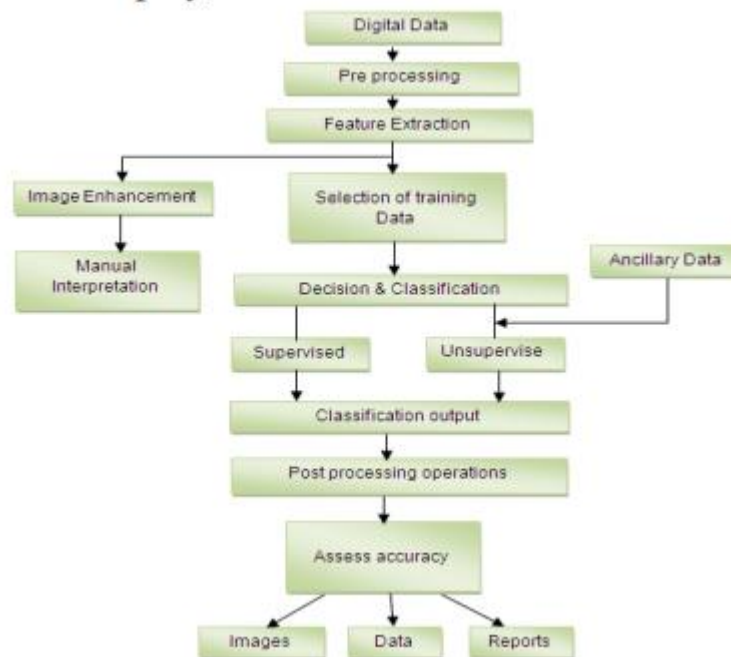


Image interpretation: to assign meaning to an ensemble of recognized objects.

Medical image computing typically operates on 2D pictures as well as 3D volumes, which are also referred to as images. These images have typical x-y-z spatial spacing and are evenly sampled data. At each sample point, data is often provided in integral form in formats like signed and unsigned short (16-bit), while formats like unsigned char (8-bit) and 32-bit float are not unheard of. The precise relevance of the data at the sampling point may change depending on the modality. For instance, although an MRI acquisition may gather T1 or T2-weighted images, a CT acquisition collects radio density measurements. During longitudinal, time-varying acquisitions, it may or may not be able to record images with regular time steps. Different representational and computational methodologies are needed for the processing of fan-like images generated by modalities like curved-array ultrasonography. Unstructured meshes like hexahedral and tetrahedral forms used in advanced biomechanical analyses are another kind of data, as are sheared images caused by gantry tilt during collection.

Segmentation

Segmentation is the process of breaking an image up into separate sections. In medical imaging, these segments often correspond to different tissue types, organs, illnesses, or other physiologically important features. Medical image segmentation is difficult due to low contrast, noise, and other imaging difficulties. Despite the fact that there are many image segmentation algorithms in computer vision, some of them have been specifically designed for use in medical image computing. The clinical knowledge that may be provided determines how the operations on the list below are carried out.

The term "biomedical image processing" is often used to describe the provision of digital image processing for biomedical sciences. Digital image processing primarily focuses on four different areas.

Each step in the creation of an image, from shooting the photo to constructing a digital image matrix, is included.

Any forms of matrix manipulation that maximize the output of the image are referred to as "image visualization."

Image analysis encompasses all post-processing steps used for numerical measurements and fuzzily interpreted biological images. Prior knowledge about the nature and content of the images is required for these techniques, and it must be thoroughly abstracted into the algorithms. Image analysis is thus a highly specialized process, and proven methods are seldom directly transferable to other application domains.

"Image management" refers to any techniques for efficiently storing, exchanging, transmitting, archiving, and retrieving image data. Hence, image management strategies also include telemedicine.

Low level processing refers to human or automated procedures that may be used without knowing in advance the particular content of a picture, in contrast to image analysis, which is frequently referred to as high level image processing. This kind of algorithm yields results that are same regardless of the content of the images. Histogram stretching, for instance, improves contrast in radiographs much as it does in any vacation photo. As a result, applications for image enhancement often use low-level processing methods.

Algorithms used for Image Processing at Different Stages

Image registration Image registration is one of the most used and GPU-implemented algorithms in medical imaging. One reason for this is the GPU's hardware support for linear interpolation, which enables very effective image and volume modification. Hastreiter and Ertl (1998) were among the first researchers to employ the GPU for image registration, mostly because of the GPU's rapid 3D interpolation speed. The CPU typically performs a parallel calculation of a similarity measure, frequently mutual information (Viola and Wells, 1997; Plum et al., 2003; Mellor and Brady, 2005), over the images, while the GPU performs a serial optimization algorithm to determine the parameters (such as translations and rotations) that produce the best match between the two images. The mutual information between two discrete variables, a and b , is defined as follows.

Edge Detection Technique

The technique of processing images that finds the edges of objects in images is known as edge detection. It searches for variations in brightness to function. Edge detection is used for image segmentation and data extraction in the domains of image processing, computer vision, and machine vision. For edge detection, algorithms like Sobel, Canny, Prewitt, Roberts, and fuzzy logic methods are often utilized. Consider the fictitious scenario of an object O that is brilliant against a dark background. As a depiction of it, the genuine item is projected onto image I . Since the object and background are contrasted, the optimum segmentation is the characteristic function IO of the object, and since there are large changes in intensity I on the border O . It seems reasonable, therefore, to define the boundary O as the set of locations where the gradient's $|I|$ norm is large. In fact, $|I|$ is a single measure whose support, if O is piecewise smooth, is exactly O . In the 1960s and 1970s, Roberts [81] and Sobel [91] developed somewhat different discrete convolution masks to estimate the gradient of digital images. The edges of these approaches are not adequately localized, and noise may distort them. Note the thick border of the heart ventricle and the presence of "spurious edges" caused by noise. Can recommended using a smoothing phase as a pre-processing step to reduce the effect of noise and a thinning step as a post-processing step to ensure that the edges are locally distinguishable. See [26] for a survey and evaluation of edge detectors using gradient techniques. Edges are defined as the zeros of $\nabla^2 I$, the Laplacian of a smooth form of the image, in psychophysics, which is where Marr and Hildreth first got the idea for their rather different approach. One may provide a heuristic explanation by assuming that the edges are smooth curves; more precisely,

Feature Extraction

Because it excels at making the prominent areas, which are often of interest, more visible, the contrast limited adaptive histogram equalization (CLAHE) approach is frequently employed in biological image processing. Each zone in the image uses local histogram equalization. The image is broken into multiple pieces. Then, the regions' boundaries are eliminated by means of a bilinear interpolation. The main objective of this method is to define a point transformation within a constrained local window, where the intensity value is assumed to be a precise representation of the local distribution of the intensity value of the whole image. It is believed that the gradual difference in brightness between the picture's centre and edges has no bearing on the local window. The point transformation distribution covers the whole intensity range of the picture and is centered on the mean intensity of the window. Think about a running sub image W with dimensions $N \times N$ and a central pixel $P(i, j)$. The picture is filtered to produce another subimage P of $N \times N$ pixels using the equation below.

Max and Min are the highest and lowest intensity values for the whole image, respectively, while μ and σ stand for the mean and standard deviation of the local window, which are defined as:

In order to provide consistent lighting across the image, this adaptive histogram equalization increases the brightness of the side that was dimly lit in the input image while leaving the well-lit side alone or decreasing its brightness.

Super-Pixel Classification using Slic Algorithm

This work uses the SLIC (simple linear iterative clustering) approach to produce super pixels in retinal fundus images. When compared to other super pixel approaches, SLIC offers great border adherence, is memory-efficient, and is speedy. The quantity of super pixels necessary is the main—and, to be honest, the only—factor influencing our use of SLIC. We developed a unique super pixel method called simple linear iterative clustering (SLIC), which uses k -means clustering to create super pixels as efficiently as possible. This algorithm is superior than other conventional strategies. Additionally, it improves segmentation speed, uses memory more quickly and efficiently, and is easy to extend to create super pixels. SLIC is simple to use and understand. The needed number of nearly equal-sized super pixels, or k , is the algorithm's single required parameter by default. To create super pixels that are about the same size, the grid interval is $S = N/k$. For color images in the CIELAB color space, k initial cluster centers = $l_i, a_i, b_i, x_i, \text{ and } y_i$ are sampled on a regular grid spaced S pixels apart as the initialization step of the clustering process. The centers are moved to the seed locations, which are located at the lowest gradient point in the neighborhood. As a result, it is less likely that a super pixel will be seeded with a noisy pixel and it won't be centered on an edge. The next step is to allocate each pixel "i" to the nearest cluster center whose search area corresponds to its location in the assignment stage. This is the key to speeding up our technique since it significantly reduces the number of distance calculations and allows us to do standard k -means clustering, which compares every pixel to every cluster center, much more quickly. This is only possible with the addition of the distance measure D , which indicates the nearest cluster centered for each pixel.

Circular Hough-Transformation

We created a plan based on the To locate minuscule circular portions in the image, we'll use a method called Circular Hough Transformation. In order to detect circles on the pictures, the circular Hough transformation is used. A collection of circular objects might be extracted from the image using this technique. The circumference of the optic disk is determined using the circle equation below.

where " r " denotes the circumference of the circle and " (a, b) " denotes the coordinates of the object's circular center. The circular disk of the picture must be located by counting votes in three-dimensional regions ($a, b, \text{ and } r$). CHT transforms the image coordinate parameters into a group of votes in the constraint space. Every dot in the group has a computation and vote tally for every conceivable combination after it. The highest vote total will decide the circle's center, and its coordinates are

II. CONCLUSION

In this work, we extracted some of the fundamental principles of medical image processing. It is important to emphasize that none of these problems has found a suitable solution, and all of the presented techniques might be significantly improved. In particular, segmentation is still a fairly haphazard process, with the best results coming from technologies that encourage active user participation. But during the last several years, developments in technology, acquisition techniques, signal processing methods, and of course mathematics have aided the field of autonomous interpretation of medical images. Curvature driven flows, which have shown to be an excellent tool for a range of image processing tasks, have surely had a substantial influence on the technical underpinning. The methodologies needed for medical imaging still involve considerable mathematical challenges across practically all of the major branches of mathematics. To sum up, we could need all the help we can get!

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